Analytic and iterative reconstructions in SPECT

J.-P. Guillement and R.G. Novikov

Analytic and iterative reconstructions in SPECT

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Numerical examples

Abstract We consider analytic and iterative reconstructions in the single-photon emission computed tomography (SPECT).

- . As analytic techniques we use Chang's approximate inversion formula and Novikov's exact inversion formula for the attenuated ray transform, on one hand, and Wiener-type filter for data with strong Poisson noise, on other hand.
- . As iterative techniques we consider the least square and expectation maximization iterative reconstructions.
- . Different comparisons are given.

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Single Photon Emission Computed Tomography (SPECT)



Г discrete subset of the set T of all oriented straight lines in the space containing the body. point of detector set Γ γ point of the space х f(x)density of radioactive isotopes a(x)photon attenuation coeff. $p(\gamma)$ projection data : number of photons coming from the body along oriented straight line γ to the associated detector

during some fixed time.

The problem : find the isotopes distribution f(x) from the projection data $p(\gamma)$ and some a priori information concerning the body (attenuation map a(x)).

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Attenuated ray transform

In some approximation the projection data \boldsymbol{p} are modeled as follows :

 $\forall \gamma \in \Gamma, \ p(\gamma) \text{ is a realization of a Poisson variate } \mathbf{p}(\gamma)$ with the mean $M\mathbf{p}(\gamma) = g(\gamma) = CP_a f(\gamma)$, all $\mathbf{p}(\gamma)$ are independent,

where $P_a f$, the attenuated ray transform of f, is

$$P_{a}f(\gamma) = \int\limits_{\gamma} \exp[-\mathcal{D}a(x,\hat{\gamma})]f(x)dx,$$

 $\hat{\gamma}$ is the direction of $\gamma,$ and $\mathcal{D}\textit{a}$ the divergent beam

$$\mathcal{D} \mathsf{a}(x, heta) = \int\limits_{0}^{+\infty} \mathsf{a}(x + t heta) dt, \; x \in \mathbb{R}^2, \; heta \in \mathbb{S}^1,$$

 $C = C_1 t$, t detection time. (The SPECT problem $p \rightarrow Cf$ has been restricted to each fixed 2D plane intersecting the body)

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Notation

. T the set of all oriented straight lines in $\mathbb{R}^2,~\mathcal{T}\approx\mathbb{R}\times\mathbb{S}^1$

.
$$\gamma \in \mathcal{T}$$
, $\gamma = (s, heta) = \{x \in \mathbb{R}^2 : x = s heta^\perp + t heta, t \in \mathbb{R}\}$

. $heta=(heta_1, heta_2)\in\mathbb{S}^1$ gives the orientation of γ

$$\theta^{\perp} = (-\theta_2, \theta_1)$$

.
$$a(x) \ge 0, f(x) \ge 0$$

- . supp a and supp f are included in a disk $B_R = \{|x| \le R\}$
- . Γ is a uniform $n \times n$ sampling of

$$T_R = \{\gamma \in T : \gamma \cap B_R \neq \emptyset\} = \{(s, \theta) \in \mathbb{R} \times \mathbb{S}^1 : |s| \leq R\}$$

The standard value for n is 128

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Problem 1. Find (as well as possible) *Cf* from *p* and *a*.

Our analytic approach to Problem 1. is based on the scheme

 $Cf \simeq P_a^{-1} \mathcal{W} p,$

where

- . \mathcal{W} is a space-variant Wiener-type filter of [Guillement-Novikov 2008] (or some analytic method for approximate finding the noiseless data g from p)
- . P_a^{-1} is a reconstruction based on some optimal combination of Novikov exact inversion formula and Chang approximate inversion formula.
 - The optimal combination is constructed via a Morozov-type discrepancy principle (minimize $||P_aCf Wp||$).

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Chang formula ([Chang 1978], [Novikov 2011]) $Cf \simeq Ch_a g$, where $Ch_{a}g(x) = \frac{P_0^{-1}(g)(x)}{w_0(x)}$ $P_0^{-1}(g)(x) = \frac{1}{4\pi} \int_{\Omega^1} \theta^{\perp} \nabla_x Hg_{\theta}(x\theta^{\perp}) d\theta,$ (FBP) $= \frac{1}{2\pi} \int_{\mathbb{S}^1} \exp[-\mathcal{D}a(x,\theta)] d\theta$ $w_a(x)$ $g = CP_a f$ (see (1) and (2)), $g_{\theta}(s) = g(s, \theta)$, *H*, Hilbert transform, $Hu(s) = \frac{1}{\pi}p.v.\int_{\mathbb{T}} \frac{u(t)}{s-t} dt$, $\mathcal{D}a$ divergent beam (3).

Chang compensation formula (4) is approximate, sufficiently stable for reconstruction from discrete and noisy data p.

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Novikov formula ([Novikov 2002])

$$Cf = \mathcal{N}_{a}g$$
, where

$$\mathcal{N}_{\mathsf{a}}\mathsf{g}(\mathsf{x}) = \frac{1}{4\pi}\int_{\mathbb{S}^1} \theta^{\perp} \nabla_{\mathsf{x}} \mathsf{K}(\mathsf{x},\theta) d\theta,$$

$$\begin{array}{lll} \mathcal{K}(x,\theta) &=& \exp[-\mathcal{D}a(x,-\theta)]\,\tilde{g}(x\theta^{\perp}),\\ \tilde{g}(s) &=& \exp\left[A_{\theta}(s)\right]\cos\left(B_{\theta}(s)\right)\mathcal{H}(\exp\left[A_{\theta}\right]\cos\left(B_{\theta}\right)g_{\theta}\right)(s) +\\ && \exp\left[A_{\theta}(s)\right]\sin\left(B_{\theta}(s)\right)\mathcal{H}(\exp\left(A_{\theta}\right)\sin\left(B_{\theta}\right)g_{\theta}\right)(s), \end{array}$$

 $\begin{array}{l} \mbox{$H$ Hilbert transform, \mathcal{D}a divergent beam,} \\ \mbox{$A_{\theta}(s) = \frac{1}{2}P_0a(s,\theta), \quad B_{\theta}(s) = HA_{\theta}(s), \quad g_{\theta}(s) = g(s,\theta), \\ g = CP_af. \end{array}$

Formula (5) is exact (for continuous case) but not very stable for reconstruction from discrete and noisy data p.

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Wiener-type filter[Guillement-Novikov 2008]

Wiener classical result Let \hat{g} , $\hat{\mathbf{p}}$, \hat{p} on $\hat{\Gamma}$ denote the 2D discrete Fourier transforms of g, \mathbf{p} , p on Γ (see (1)). Let \mathcal{W} denote a space-invariant linear filter on Γ that acts in the frequency domain as

$$\hat{u}(j) \to \hat{W}(j)\hat{u}(j), \quad j \in \hat{\Gamma}, \\ \hat{W} \text{ is real - valued, } \quad \hat{W}(j) = \hat{W}(-j),$$

where \hat{W} is the window function of \mathcal{W} . **Then** the mean $\mu(\mathcal{W}, g) = M \|\mathcal{W}\mathbf{p} - g\|_{L^2(\Gamma)}^2$ is minimal with respect to \mathcal{W} iff

$$\hat{W}(j) = \hat{W}^{opt}(j) \stackrel{\text{def}}{=} rac{|\hat{g}(j)|^2}{|\hat{g}(j)|^2 + V}, \ \ j \in \hat{\Gamma}, \ V = n^{-1}\hat{g}(0) = n^{-2}\sum_{\gamma \in \Gamma} g(\gamma),$$

where n is the sampling number. But formula (6) contains unknown g. and iterative reconstructions in SPECT J.-P. Guille-

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Regularization of \mathcal{W}^{opt} Let S_1, \ldots, S_{n^*} a partition of $\hat{\Gamma}$ such that $-S_{\alpha} = S_{\beta_{\alpha}}$. Let a filter \mathcal{W} that acts in the frequency domain as

$$\hat{u}(j) \rightarrow \hat{W}(j)u(j), \ \ j \in \hat{\Gamma}, \ \hat{W} \ \ ext{is real} - ext{valued}, \ \ \hat{W}(j) = \hat{W}(-j), \ \hat{W} \ \ ext{is constant on each } S_{lpha}$$

Then $\mu(\mathcal{W},g) = M \|\mathcal{W}\mathbf{p} - g\|_{L^2(\Gamma)}^2$ is minimal with respect to \mathcal{W} iff

$$\hat{W}(j) = \hat{W}^{r.o.}(j) \stackrel{\text{def}}{=} \frac{\sum_{g,\alpha(j)}}{\sum_{g,\alpha(j)+V}}, \quad j \in \hat{\Gamma},$$

$$\sum \frac{\det}{\sum} \frac{1}{|\hat{\sigma}(i)|^2} \propto -1 \qquad n^*$$

$$\mathcal{I} = n^{-1}\hat{g}(0) = n^{-2}\sum_{\gamma \in \Gamma} g(\gamma),$$

. $|\mathcal{S}_{lpha}|$ number of elements in \mathcal{S}_{lpha}

. $\alpha(j)$ denotes α such that $j \in S_{\alpha}$

Note : If $S_{\alpha(j)} = \{j\} \ \forall j \in \hat{\Gamma}$, then $\mathcal{W}^{r.o.}$ is reduced to \mathcal{W}^{opt} .

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Approximation result The window

$$\hat{A}(j) = \begin{cases} \frac{\sum_{p,\alpha(j)} - V_p}{\sum_{p,\alpha(j)}} & \text{if } \sum_{p,\alpha(j)} - V_p > 0\\ 0 & \text{if } \sum_{p,\alpha(j)} - V_p \le 0 \end{cases}$$
$$\sum_{p,\alpha} = \frac{1}{|S_{\alpha}|} \sum_{i \in S_{\alpha}} |\hat{p}(i)|^2,$$
$$V_p = n^{-1} \hat{p}(0) = n^{-2} \sum_{\gamma \in \Gamma} p(\gamma),$$

is a very efficient approximation to $\mathcal{W}^{r.o.},$ under the condition that

 $|S_{\alpha(j)}|$ is great enough in comparison with |j| (7)

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$$\mathcal{A}^{simp}$$
: $S_{\alpha(j)} = \{j\}$. (7) is not fulfilled.
 \mathcal{A}^{1d} : $S_{\alpha(j)} = \{z = (z_1, z_2) \in \hat{\Gamma}, z_1 = j_1\}$. (7) is fulfilled. \mathcal{A}^{sym} : $S_{\alpha} =$ squares centered at 0 in $\hat{\Gamma}$.
(7) is fulfilled.Image: Comparison of \mathcal{A}^{sym} , uses space-invariant considerations in $l_1 \times l_2$ neighborhood of each detector $\gamma \in \Gamma$. In our numerical examples $l_1 = l_2 = 8$.

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Optimized analytic reconstruction (OAR)

$$Cf \simeq Cf_{lpha} = \mathcal{N}_{a_{lpha}}(\mathcal{W}p)_{lpha} + \mathcal{C}h_{a}(\mathcal{W}p - (\mathcal{W}p)_{lpha})$$

where

- . \mathcal{N}_a and $\mathcal{C}h_a$ are the inversion operators of formulas (5) and (4),
- . \mathcal{W} is a space-variant Wiener-type filter of [Guillement-Novikov 2008],
- . $(\mathcal{W}p)_{\alpha}$ and a_{α} are the low-frequency parts of $\mathcal{W}p$ and a, obtained via some standard 2D space-invariant filtering dependent on α ,
- . α is an optimization parameter choosed to minimize the discrepancy $||P_aCf_{\alpha} Wp||_{L^2(\Gamma)}$.

The ansatz Cf_{α} of (8) is motivated by the facts that $\mathcal{N}_a p$ of the exact formula is sufficiently stable on sufficiently low frequency part of p and a, whereas $Ch_a p$ of the Chang approximate formula is sufficiently stable on reasonably high frequency part of p and a.

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Gradient

Find f wich minimizes $||P_a f - p||_{L^2}^2$, with p the projection data. In discrete model, this corresponds to Find $X = \{f(x_i)\}$ that minimizes $\Phi = 1/2||AX - Y||_2^2$

. A the matrix corresponding to P_a

. Y the vector formed by the projections $p(\gamma)$.

It is a quadratic least square problem which can be treated by the gradient method, the conjugate gradient... In addition, to avoid adjustment of the noise, one can add a term for regularization like $\alpha \Lambda f.f.(\Lambda = -Laplacian)$ or filter the data. The gradient iterations are

$$X' = X - \rho d_0, \quad d_0 = \nabla \Phi = A^* (AX - Y), \ \rho = \frac{\|d_0\|^2}{A^* A d_0.d_0}.$$

AX and A^*Z are computed as

$$\begin{array}{l} AX(s,\theta) = \int e^{-\mathcal{D}_a(x(t),\theta)} X(s\theta^{\perp} + t\theta) dt \\ A^*Z(x) = \int e^{-\mathcal{D}_a(x,\theta)} Z(x\theta^{\perp},\theta) d\theta \end{array}$$

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Expectation Maximization (EM)

EM is a parameter adjustment method by maximum likelihood principle. Introduced by [Shepp-Vardi 1982] in emission tomography PET, the algorithm is designed to compute the maximum of the probability L(p|f) so that the emission map fgenerates the projections p. For that, one consider a discrete model for which f(x) and $p(\gamma)$ are Poisson distributions. EM iterations for the maximum are simple and give good results in SPECT. OSEM (Ordered Subsets EM) [Hudson-Larkin 1994] accelerates the EM iterations by limiting back-projection computation on "ordered" subsets of projections.

EM iterations Start with $f_0 \equiv 1$. Iteratively

. compute $p_n = P_a f_n$ and compare to supplied projections p by

$$q_n = \frac{p}{p_n}$$

. update f estimation by

 $f_{n+1}(x) = f_n(x) \int e^{-\mathcal{D}_a(x,\theta)} q_n(x\theta^{\perp},\theta) d\theta \frac{1}{\int e^{-\mathcal{D}_a(x,\theta)} d\theta}$

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Space-variant Wiener filter $A_{8,8}^{sym}$ and O.A. reconstruction



 $\mathsf{OAR}: \|r - r_0\|_2 / \|r_0\|_2 = 36\%$



Spectrum



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Space-variant Wiener filter $A_{8,8}^{sym}$ and O.A. reconstruction



Projections $\|\tilde{p} - g\|_2 / \|g\|_2 = 10\%$



Spectrum



 $\mathsf{OAR}: \|r - r_0\|_2 / \|r_0\|_2 = 22\%$



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Gradient : $||r - r_0||_2 / ||r_0||_2 = 24\%$



Profile





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